Analyse fractale, analyse temps/fréquence

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FDpV for other models

The FDpV method is general, and can be adapted to more complex models:

- the Toy Model: Sequence of independent r.v.
 - Changes on the mean (BGF, 2011);
 - Changes on the variance (BGF, 2011).
- 2 Linear Regression
 - Changes on the slope (BGF, 2011);
 - Changes on the intercept (BGF, 2011).
- Fractal like processes
 - Changes on the Hurst index;
 - Changes on the variance.

Detection of change points in the slope

Data

- **1** n = 1400
- **2** $\Delta = 1, \, \sigma = 30$
- $\nu_k \in [3, 5]$ where $\nu_k := |a_k a_{k+1}|$.

Calibration of the FDp-V method

- **9** $p_1^* = 0.05$,
- 2 $p_2^* = 10^{-5}$
- A = 100







Smaller change points

Data

- **1** n = 1400
- 2 $\Delta = 1, \sigma = 30$
- **3** $\nu_k \in [0.75, 1].$

Calibration of the FDp-V method

- **1** $p_1^* = 0.05$
- 2 $p_2^* = 10^{-5}$
- A = 100





In this section, we propose more elaborated model for biological series than the toy model of sequence of independent Gaussian r.v. with piecewise constant mean and variance.

We will investigate the two following dynamical models:

- Locally stationary Gaussian process;
- Fractal process being piecewise fBm (work in progress, see PhD thesis Mehdi Fhima).

- " Heartbeats, hormones and health: is variability the spice of life?"
- Goldberger (2001) American J. Critical Care Medicine 163, 1289–1290.
- Ivanov C., Amaral L., Goldberger A.L., Havlin S., Rosenblum M.G., Struzik Z. R., Stanley H. E.(1999). Multifractality in human heartbeat dynamics. *Nature* 399.

Recall on stationary Gaussian process

Such a process has the following spectral representation (Cramér):

$$X(t) = \mu + \int_{R} e^{it\xi} f^{1/2}(\xi) \, dW(\xi), \quad \text{for all} \quad t \in R, \qquad (1)$$

where

- *dW* is a complex Wiener measure chosen such that *X* is real value;
- the power spectral density *f*(ξ) is a non negative even function. Moreover Formula (1) is well defined under the condition

$$\int_{R} f(\xi) \, d\xi < \infty.$$

Fractional Brownian motion and Gaussian process with stationary increments

- Fractional Brownian motion (fBm) has been introduced by Kolmogorov (1940) and popularized for its relevance in application by Mandlebrot & Van Ness (1968).
- FBm is a particular case of zero mean stationary Gaussian process with spectral representation:

$$X(t) = \int_{R} (e^{it\xi} - 1) \cdot f^{1/2}(\xi) \, dW(\xi), \quad \text{for all} \quad t \in R, \ (2)$$

corresponding to a linear spectral density:

$$\log\left(\!f(\xi)\right) = -(2H+1)\log(|\xi|) + \sigma^2$$

where *H* is the Hurst index and σ a scale parameter (variance).

FBm and Gaussian process

• The spectral density of fBm is an affine function of frequency (log-log), and this corresponds to the self-similarity of fBM.

Following Mandelbrot, an important feature of f.B.m. is "the concept of self-similarity, a form of invariance with respect to changes of time scale."

• Formula (2) is well defined under the condition

$$\int_{R}\left|e^{it\xi}-1\right|^{2}\cdot f(\xi) \,\,d\xi<\infty.$$

• Self-similarity implies affinity (log-log scale) of spectral density, then

$$\int_{R} \sigma^{2} \left| e^{it\xi} - 1 \right|^{2} \cdot |\xi|^{-(2H+1)} d\xi < \infty,$$

r $H \in (0, 1)$

and after $H \in (0, 1)$.

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Spectral density of FBm



Spectral density of Multiscale FBm, to be continue



Multiscale FBm

- FBm is a particular case of Gaussian process with stationary increments depending on two parameters: *H* ∈ (0, 1) and *σ* > 0.
- In some applications (see Bardet & Bertrand 2007), we find Hurst index $H \notin (0, 1)$.

This paradox is solved by the multiscale fBm, which is still a zero mean stationary Gaussian process, but with a piecewise affine spectral density (log-log scale) (Bardet & Bertrand, 2007b)

Spectral density of Multiscale FBm



Cardiologist point of view

Cardiologists are interested in the study of heartbeats series in two frequency bands:

- The hight frequency (HF) bands (0.15 Hz, 0.5 Hz) assumed to reflect regulation by the orthosympathetic system.
- The low frequency (LF) bands (0.04 Hz, 0.15 Hz) assumed to reflect regulation by the parasympathetic system.

Task force of the European Society of Cardiology and the North American Society of Pacing and Electrophysiology (1996).

ECG and Tachogram



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Statistical estimation of spectral density

In Bardet & Bertrand (2010), we have made an estimation of the spectral density of heartbeat series for a shift worker (C1) by wavelet analysis.



Figure: spectral density (log-log plot) of C1, at work

Statistical estimation of spectral density following the activity



Figure: spectral density (log-log plot) of C1, at rest

Statistical estimation of spectral density following the activity



Figure: spectral density (log-log plot) of C1, sleeping

Locally stationary Gaussian process

Such a process has the following spectral representation (Cramér):

$$X(t) = \mu(t) + \int_{R} e^{it\xi} f^{1/2}(t,\xi) \, dW(\xi), \quad \text{for all} \quad t \in R, \quad (3)$$

where

- *dW* is a complex Wiener measure chosen such that *X* is real value;
- the spectral density *f*(*t*, ξ) is a piecewise constant function of time, i.e., there exists a partition τ₁,..., τ_k such that *f*(*t*, ξ) = *f*_k(ξ) for *t* ∈ [τ_k, τ_{k+1}[;
- the mean $\mu(t)$ is also piecewise constant for another partition $\tilde{\tau}_1, \ldots, \tilde{\tau}_L$ with $\mu(t) = \mu_\ell$ if $t \in [\tilde{\tau}_\ell, \tilde{\tau}_{\ell+1})$.

Statistical analysis of orthosympathetic and parasympathetic frequency bands

We calculate the wavelet coefficient in HF and LF bands,

$$W_{\psi_j}(b) = \int_{\mathbb{R}} \psi_j(t-b) X(t) dt$$
 for $j = 1$ or 2. (4)

where the wavelet ψ_j has a frequency support well localized in the HF or LF frequency band, with time support L_j

- We calculate the corresponding log-wavelet energies.
- We use FDpV method to segment log-wavelet energies.

Statistical analysis of HF and LF frequency bands (Mathematical formulas)

• The harmonizable representation of wavelet coefficients (Bardet & PRB 2010 or Ayache & PRB 2011)

$$W_j(b) = \int_R e^{ib\xi} \widehat{\psi}_j(\xi) f_k^{1/2}(\xi) \, dW(\xi)$$

for all $(b, b + L_j) \subset (\tau_k, \tau_{k+1})$.

• Thus $W_j(b)$ is a zero mean complex valued Gaussian process with variance $E(|W_j(b)|^2) = \int_R |\widehat{\psi}_j(\xi)|^2 f_k(\xi) d\xi$ where |z| denotes the modulus of the complex number z.

In Vivo Tachogram Analysis (In ViTA)

By using software "InViTA", we get for shift worker Y1



4) An index of well-being

Heartbeat series for a Marathon runner (B1)



Data furnished by V.Billat and LEPhE (laboratory of exercise physiology, INSERM and Évry Genopole).

In Vivo Tachogram Analysis (In ViTA) for Marathon runner B1

Changes detection on heart frequency of B1 Paris Marathon 2006 Time resolution = 3 minutes-15 seconds. Detection threshold = 2 beats by minute The number of change points is 96



Conclusion

New data, new models and new statistical methods allow new applications to be developed:

- New devices can record high frequency physiological signals inside and outside the laboratory. These signals are digital, indexed by time, fluctuating and with big data size.
- Generalizations of the fractional Brownian motion with Hurst index varying have been introduced since 1996, and several statistical estimators have been proposed.
- Change point analysis can accurately describe time varying parameters. However big datasets also require to control the numerical efficiency of statistical procedures.

- Bertrand, P.R., Fhima, M. and Guillin, A. (2011) "Off-line detection of multiple change points with the Filtered Derivative with p-Value method." Sequential Analysis 30 (2): 172-206.
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